ANIMA: Non conventional Brain Computer Interfaces in Robot Control through Electroencephalography and Electrooculography, ARP Module

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ABSTRACT

ANIMA has as a primary objective to compare three non conventional human computer interfaces that comply with the industrial robot ST Robotics R-17 instructions. This module, Alpha Waves Related Potentials -ARP-explains how brain waves are obtained, processed, analyzed and identified depending on their frequency. This module makes use of the Open EEG Project's open hardware monitor for brain wave activity, called the modular EEG. The brain waves are obtained through an electrode cap complying with the international 10-20 system for electrode positioning. The brain waves are processed with a fast Fourier transform using a microcontroller and analyzed in software identifying the alpha wave's contribution. A program identifies the amount of time that alpha wave generation was maintained through concentration, and instructions are sent to the robotic arm, executing one of four pre-defined routines. Thirty percent of the users attained control over the robotic arm with the human computer interface.

Keywords: Electronics, Fast Fourier Transform, microcontrollers, Electroencephalography, Neurocontroller.

1. Introduction

Brain waves can be obtained through electroencephalography –EEG- using an electrode cap. The electrodes obtain the brain's electrical variations caused by the neuronal interaction. To be able to observe potentials (micro volts scale) from a specific region of the brain, a comparison between two electrodes is needed; one at an area of reference and the other at the area of interest. The international system 10-20 for electrode positioning was created to standardize the position of electrodes in areas of interest.

Brain waves are classified according to their frequency; delta (0.2-3.5 Hz), theta (3.5 - 7.5Hz), alpha (7.5 -13Hz), beta (13-28Hz) and gamma (28-40Hz) (Johnston, 1997). Beta can be divided in two regions: Beta 1 or beta Low (13-20.5 Hz) and beta 2 or beta High (20.5 a 28 Hz).

Alfa waves are produced in moments of relaxation and tranquility. Most people can produce them when they close their eyes and relax. However, maintaining the generation of alpha waves with eyes wide open is not an easy task (Johnston, 1997).

Alpha waves are one type of brain waves detected by electroencephalography –EEG- and predominantly originate from the occipital lobe or parietal lobe during wakeful relaxation with closed eyes. Alpha waves are reduced with open eyes and drowsiness and sleep.

The graphic representation of the Fast Fourier Transform -FFT- of a wave is a diagram named Fourier spectrum in which the frequency and magnitude of each sinusoid component is represented (Díaz-López, 2009). This transform is used to transform a signal from the time domain to the frequency domain. Thus, the acquired brain waves can be classified according to their frequency. Even dough, the FFT is not a state of the art signal-processing algorithm like PCA, ICA, wavelets or multivariable statistical analysis it's still valid for an initial approach.

ANIMA project has three different modules: the ocular module, motor module and the alpha wave related potentials module –ARP-. All modules were financed by CONCYT (National Council for Science and Technology, for its Spanish abbreviation). Each module makes its own implementation for moving the robotic arm R17; signals produced by the changes in the electric field of the eyes caused by their movement (Valdeavellano, 2009), brain waves related to motor tasks (Martínez, 2009) and brain waves related to alpha activity. Comparison between the three modules could be done in terms of effectiveness and speed for controlling a Robotics R17 robotic arm. Research in this country is starting to flourish in this area and projects like this one are the very first steps.

2. EXPERIMENTAL DESIGN

Brain waves on the parietal lobe are amplified, filtered, sampled and digitalized using the open hardware of the "Open EEG Project" (Open EEG Project, 2008) for brain wave acquisition. Brain waves were analyzed by applying the FFT to identify the frequencies involved with concentration. The signals are analyzed using a Python (Python Software Foundation, 2010) software application to identify the alpha waves produced by concentration. This software identifies the contribution of the theta, alpha, beta1 and beta2 to the frequency spectrum on the FFT. The application uses the alpha waves contribution to identify alpha waves concentration.

Finally, the same application sends instructions to the robotic arm according to the amount of time the user maintained the alpha concentration, thus, executing one out of the four predefined routines for the R17.

3. METHODOLOGY

Figure 1 shows the four main steps for this paper. These four steps will be explained on the following sections.

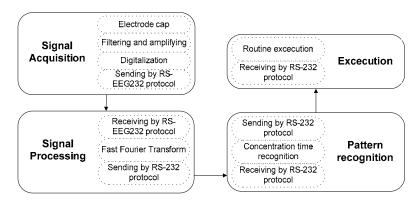


Figure 1. Steps for the ARP module.

3.1 SIGNALS ACQUISITION

An electrode cap complying with the IS 10-20 was used to obtain the brain waves. Electrodes used were P3 and GND as the reference. A modular EEG was built which has two printed circuit boards –PCBs-, one analog for

amplification and filtering, and one digital for communication with a PC. The design for both PCBs is available on the Open EEG Project webpage. The modular EEG PCBs were manufactured at the University and bought in Olimex (Figure 2) at the same time (OLIMEX Ltd, 2009). PCBs from both manufacturers were compared and the same results were obtained. An application was made using Python to calibrate the gain obtained with the PCBs.

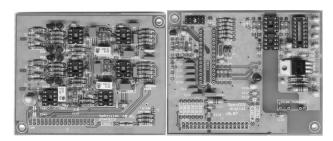


Figure 2. Digital and analog PCB for Open EEG Projects modular EEG(Open EEG Project, 2008).

3.2 SIGNAL PROCESSING

The FFT was calculated in a dsPIC microcontroller obtaining data from the modular EEG (AVR microcontroller) communicating through the RS-232EEG protocol and sending the results through RS-232 protocol to a PC (Figure 3).

A dsPIC microcontroller with two RS-232 (UART) communication ports was used with a 10MHz 8xPLL, therefore the dsPIC could work at 80MHz. This allows the dsPIC to receive data from the modular EEG at 57600 baud and send new data to the PC at 115200 baud. This speed is needed so the FFT can be calculated and the data can be sent to a PC in real time. A 256-byte array is sent containing information about the frequency spectrum (magnitude for the 0-128 Hz range) with 1 Hz resolution.

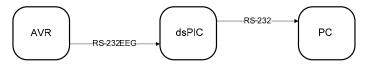


Figure 3. Communication between the Modular EEG boards and PC.

3.3 PATTERN RECOGNITION

An application was developed using Python to receive the dsPIC data over RS-232 protocol. The application discards the data related to frequencies above 30 Hz. The remaining region was divided into frequency regions according to brain waves classification: theta, alpha, beta1 and beta2. For each region an integral of the spectrum was computed. From these integrals the normalized contribution percentage was calculated.

On the GUI (Graphic User Interface) a graph presents the normalized contribution percentage for the four frequency bands (Figure 4).

Using this application the brain waves are processed comparing the P3 and GND electrode positions from the IS 10-20 cap to identify concentration periods. For a period to be valid there are two requirements: the normalized contribution percentage for alpha waves must be above a threshold of 40 percent (0.4), and a difference of normalized contribution percentage of at least 20 percent (0.2) between alpha waves and the other brain waves (theta, beta1 and beta2) must be obtained. The application identifies concentration periods of 4, 6, 8 and 10 seconds.

The application generates different sounds (beeps) for each identified period. The sound acts as a feedback to the user because it is easier to achieve alpha state with closed eyes.

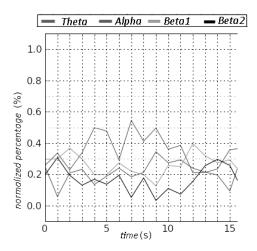


Figure 4. Normalized percentage shown on the Python GUI.

3.4 EXECUTION

The GUI described in the previous section identifies alpha concentration periods of time. Another application was developed for the GUI to communicate with the robotic arm R17. This application has two goals: to send an order on each identified period and translate that order to the R17 programmed routines.

Each alpha state period of time was mapped to a R17 routine (Table 1.). The application contains defensive programming to prevent the R17 from going off its limits of movement.

Table 1. Called routine for each alpha state period.

Seconds	Routine
4	Forward
6	Backward
8	Right
10	Left

4. RESULTS

Figure 5 shows a snapshot of the final application where the real time FFT is on the top and the graph of the normalized percentage is on the bottom. The real time FFT output is shown in Figure 6. This Figure shows a zoom in of the application using a 14Hz square wave signal as input.

The bottom of the GUI application is shown in Figure 7. In this figure it can be seen that the two required conditions discussed on the previous section are reached after 10 seconds. The thick line on 40 percent stands for the threshold of alpha waves and the 20 percent separation can be easily seen too. The times set for each task are based on various preliminary tests to assure that the alpha waves are being generated voluntarily and are not small involuntary periods of alpha wave generation. After generating alpha waves for a particular task the subject needs to generate 8 seconds of cumulative non-alpha waves to confirm the task, then the subject can start a new period of alpha wave generation and choose a different task.

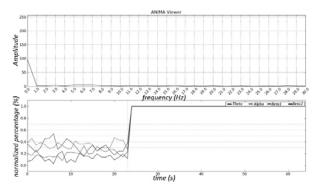


Figure 5. Python application GUI with real time FFT and normalization percentage of brain waves.

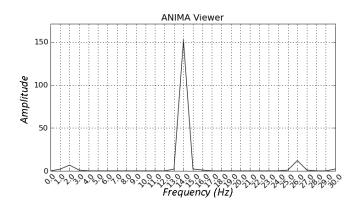


Figure 6. FFT for a 14 Hz square wave signal.

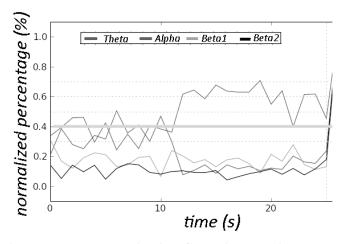


Figure 7. Python application GUI with real time FFT.

Tests were made on twenty seven subjects, nine females and eighteen males (Table 2). Testing subjects were asked to close their eyes and then start counting from 1 to 10 until they listened to the first beep. If they achieved this, the second test was to achieve the fourth beep, else the test was ended. Subjects who achieved the fourth beep were able to successfully control all the tasks. In some cases the subject was not able to control the fourth beep (Task 4) but was able to control the other three tasks (Table 5). The order of appearance in Table 5 follows the order of the tests trial.

Table 2. ARP control test of success.

Subjects	Yes	No
All	29.63%	70.37%
Men	38.89%	61.11%
Women	11.11%	88.89%

In Table 2 the success in the test is defined as the subject who can control the four tasks, the rest was considered as a failure.

In Table 3 the success for each task is shown. Males show equal difficulty in achieving the tasks two, three and four; either they achieved full control or just achieved to control the first task. It's interesting that women display a much bigger trouble achieving the fourth task. Also the percentage of women who accomplished task 1 is lower. This can be visually verified in Figure 8.

Table 3. Tasks test of success.

Subjects	Task 1	Task 2	Task 3	Task 4
All	55.56%	33.33%	33.33%	29.63%
Men	61.11%	38.89%	38.89%	38.89%
Women	44.44%	22.22%	22.22%	11.11%

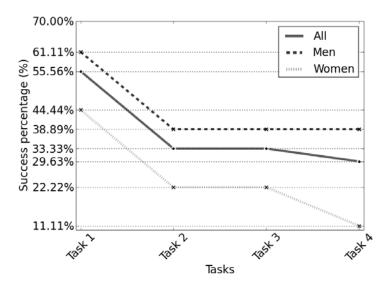


Figure 8. Success percentage in task tests for women, men and all subjects.

Table 4 shows the improvement showed on the subjects that didn't achieve all four tasks. Improvement is successful if they managed to accomplish at least one task, in case they started without managing any. Women and men have similar percentage of improvement, around 37 percent, which suggests that improvement doesn't depend on the skill to sustain alpha wave generation. This also suggests that subjects could manage the ARP control with proper training (Palke, 2003), but further studies are required to verify these hypotheses. It's interesting to notice that based on some additional tests, it was observed that alpha waves are affected by group pressure, or any distraction, e.g. music, people talking, or strong noises.

Table 4. Unsuccessful subjects that showed improvement.

Subjects	Yes	No
All	36.84%	63.16%
Men	36.36%	63.64%
Women	37.50%	62.50%

Table 5. ARP control test results.

Subject	T1	T2	Т3	T4	Woman	Man
Subject 01	YES	YES	YES	YES		X
Subject 02	NO	NO	NO	NO	X	
Subject 03	NO	NO	NO	NO	X	
Subject 04	NO	NO	NO	NO		X
Subject 05	YES	NO	NO	NO		X
Subject 06	YES	YES	YES	YES		X
Subject 07	YES	YES	YES	YES		X
Subject 08	NO	NO	NO	NO		X
Subject 09	YES	YES	YES	YES		X
Subject 10	YES	NO	NO	NO	X	
Subject 11	YES	YES	YES	NO	X	
Subject 12	YES	YES	YES	YES		X
Subject 13	NO	NO	NO	NO	X	
Subject 14	NO	NO	NO	NO	X	
Subject 15	NO	NO	NO	NO		X
Subject 16	NO	NO	NO	NO		X
Subject 17	YES	NO	NO	NO		X
Subject 18	NO	NO	NO	NO		X
Subject 19	YES	YES	YES	YES		X
Subject 20	YES	NO	NO	NO		X
Subject 21	NO	NO	NO	NO	X	
Subject 22	YES	NO	NO	NO	X	
Subject 23	NO	NO	NO	NO		X
Subject 24	YES	NO	NO	NO		X
Subject 25	YES	YES	YES	YES		X
Subject 26	YES	YES	YES	YES	X	
Subject 27	NO	NO	NO	NO		X
					9	18

^{*}T = Task

5. CONCLUSION

The hardware and software proposed implements a BCI to control the robotic arm R17 using alpha waves concentration by means of open EEG hardware and software developed at a local University.

Thirty percent of the users were able to control the robotic arm through the ARP module. Thirty seven percent of the testing subjects showed an improvement on the BCI control.

The system is to be used as a base for a much complex BCI, as for now it represents the beginning of a nonconventional method of robot control that can be applied to different fields of study. The industrial robotic arm was just used to test the BCI, but it could be applied to any other machine or interface that complies with four basic movements.

The purpose of the entire application is to offer a neuro-feedback system that could be used to help handicapped people, but its actual state is still too basic.

6. FUTURE WORK

The project could use neuronal networks to recognize patterns for specific activities such as spacial and mathrelated activities, nevertheless results are not guaranteed.

The developed Python application can be used to make an exhaustive analysis of the brain waves. Data such as hemisphere asymmetry, normalized spectral contribution on each hemisphere, peak frequency and mean spectral area could be used as features. These data can be applied to a selection algorithm to identify which ones can be used for identifying a pattern. Then, a Bayesian Network classifier can be used to distinguish between each task (Lee and Tan, 2006) (Keirn and Aunon, 1990).

The use of gamma brain waves to determine high-stress states can be applied to avoid sending commands to the robotic arm and wait until the subject is back to the relaxed state so that commands can continue to be sent.

Some patterns could be found among non-standardized parameters using energy measurements of the spectrum (alpha, beta, theta, delta and gamma).

Mathematical tools like PCA, ICA, wavelets and multivariable statistical signal processing should be used to improve the processing algorithm.

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